

Terahertz Imaging in Biomedical Detection: Principles, Applications, and Challenges

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Abstract: Terahertz (THz) imaging has emerged as a powerful technique with great potential for biomedical applications. This review focuses on its rationale, strengths, limitations, and recent advances. Terahertz imaging, with low photon energy, enables non-ionizing and non-invasive detection. Terahertz is sensitive to temperature, polar molecules such as water, and hydrogen bonds. Cancerous cells have loose structures, higher water content, and more united vibrational properties than healthy cells. Therefore, THz imaging is susceptible to malignant tissues. Complementary techniques such as nanoparticle injection, thermal modulation (heating and freezing), and methylation can improve THz imaging's ability to detect breast cancer, epidermoid carcinoma, gastric cancer, diabetes, and skin cancer(melanoma). However, it still faces challenges, e.g. limited penetration depth, low signal-to-noise ratio, and slow acquisition speed. Advances in terahertz metallic tips, single-pixel cameras, offer new insights for overcoming these limitations. The paper also mentioned the convergence of terahertz imaging with other techniques, named hybrid systems, and the development of new data processing methods. Overall, terahertz imaging has the potential to revolutionize biomedical diagnosis and treatment.

Keywords: terahertz imaging, cancer detection, water content, nanoparticles

1. Introduction

Terahertz (0.1-10 THz) imaging is a potent answer to the increasing need for advanced imaging tools. THz imaging is comprehensively noninvasive and sensitive compared to traditional imaging tools such as X-ray, CT, and MRI. With its low photon energy (0.4 to 41 meV) [1], THz is unable to ionize the atoms or damage the DNA, making it suitable for in vivo detection. THz can detect the subtle difference of polar molecules. From a biomedical perspective, THz highlights the deviance of water content in body tissues [2], which is used to distinguish abnormal parts like cancerous cells. Although the limited penetration depth of in vivo tissues limits the diagnostic precision, enhancements such as nanoparticles and hybrid detection [3] could improve the range and specificity of detection.

This paper aims to find the application of terahertz imaging and its limitations. The imaging method has disadvantages of high response to disturbance, low resolution, slow acquisition speed, small sample size, and lack of standardization. This paper helps reveal the current advantages of terahertz imaging and its future target. If the use of terahertz imaging in clinical practice is popularized, it would gain more experimental data and doctors' attention to improve this technology in the future.

2. Principle

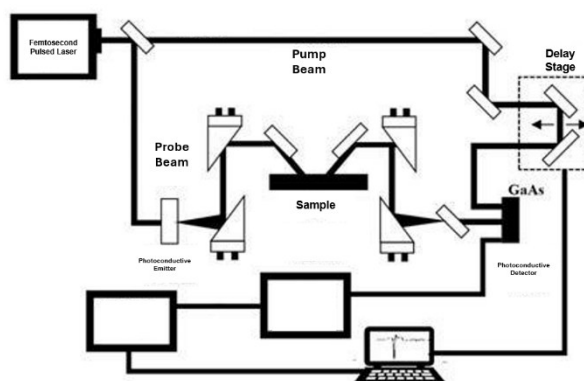


Figure 1: Pulsed wave THz imaging system using photoconductive antennas in a reflection-based geometry

THz imaging has two detection systems: the continuous wave system (CW) and the terahertz pulsed imaging system (TPI). CW maintains certain (one to several) frequencies and analyzes the difference in absorption between healthy and cancerous cells, while TPI detects the boundaries between tissues through transmission or reflection of the surface and the change of the pulse (delay, amplitude, and phase). Both act as the base of the THz imaging. Figure 1 indicates the pulsed wave THz imaging system, which is more widespread in experiments for its high spatial resolution [3]. For clinical applications, continuous wave THz has more potential. Their performance advantages are mentioned in Table 1 [3].

Table 1: Comparison of terahertz imaging technology performance

Performance	Pulse wave THz imaging system	Continuous wave THz imaging system
Penetration depth	Relatively weak	Relatively strong
Spatial resolution	Higher, up to about 1.0mm	Limited, approximately 2.5mm-2.6mm
Acquisition speed	Slower	Faster and capable of real-time imaging

THz imaging detects the motion (vibration, rotation, oscillation) of molecules and hydrogen bonds. The longer the wavelength, the less scattering and noise [4]. The higher the frequency of THz bandwidth, the clearer the molecular interstices of DNA and proteins [5]. THz imaging is perfect balance. Water molecules, which are abundant in bio tissues, absorb the THz radiation drastically, causing both its high sensitivity and limited penetration.

As most cancer starts on soft surfaces in the body, they have loose structures, higher water content, and more united vibrational properties($\sim 1.65\text{THz}$) than normal tissues [6]. These properties distinguish the health cells from the cancerous cells, acting as a biomarker of cancer. The penetration depth fluctuates from microns to millimeters, depending on the percentage of fat, water, and proteins [7].

3. Application

3.1. Breast cancer (invasive ductal carcinoma, IDC)

For breast cancer, operations are required to remove the cancerous tissue with high precision to ensure safety and preserve healthy tissues. THz are used to identify the magnitude and frame of the tumor area with different refractive indices, and it is clear enough to distinguish the fat, fibrosis, and cancer in the breast [8]. Figure 2 shows different transition areas of a sample between normal breast cells and cancerous cells. The breast cancer is named triple-negative invasive ductal carcinoma, labeled IDC. There is consistency between the upper images (ex vivo) labeled IDC and the lower images (in vivo) that are orange to dark red. This THz imaging can successfully distinguish normal breast tissue from cancerous tissue.

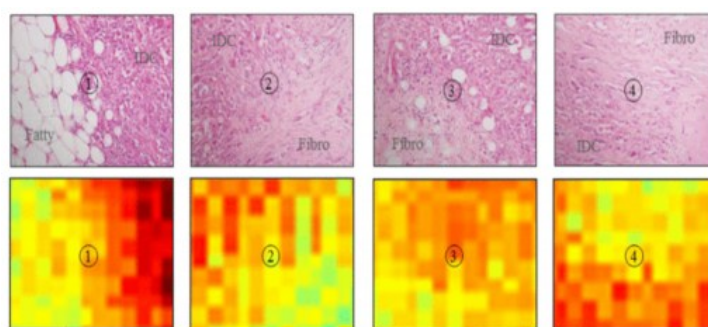


Figure 2: The THz reflection imaging of different parts of a sample with triple-negative invasive ductal carcinoma (IDC), a type of breast cancer. Upper ①: The transition areas between IDC and normal tissues (Fatty); Upper ②, ③, ④: The transition areas between IDC and normal tissues (Fibro); Lower ①, ②, ③, ④: THz reflection images of the sample parts above

3.2. Epidermoid carcinoma

For epidermoid carcinoma, gold nanorods are used in THz imaging. The specificity of THz imaging is raised by the difference in heat. The near-infrared laser (NIR) emits electromagnetic waves, penetrating through the target area. Gold nanorods block the waves and absorb the radiated energy to raise the temperature. Gold nanorods are distributed linearly with the water content, while cancerous tissues contain higher percentages of water. Thus, the temperature of cancerous tissues is higher than normal tissues under THz imaging. A minute change in temperature is enough to intensify THz signals, which improves the comparison and clarifies the THz imaging [9].

3.3. Gastric cancer

For gastric cancer, Gadolinium Oxide Nanoparticles (GONPs) improve diagnosis by targeting the cancer cells with antigens and antibodies. Gadolinium absorbs electromagnetic waves up to 3 times more than water molecules. GONPs delay pulses in phase and decrease the peak intensity [10]. These traits exemplify the distinction between gastric cancer with the presence of GONPs and normal tissue, which resolves the tumor margins in THz imaging.

3.4. Diabetes

For diabetes using ex vivo method, THz effectively analyzes the gas content from the dried blood and kidney samples [11]. For in vivo application, THz noninvasively detects the skin structure, subsurface blood flow, and the glucose concentration with 95% accuracy [12].

3.5. Skin cancer (melanoma)

3.5.1. Freezing method

Researchers can freeze the tissue to improve the quality of THz detection for skin cancer, especially melanoma. The change in states increases the depth of penetration in THz, as ice is more permeable compared to water. The contrast between melanoma and non-melanoma skin cells is also increased, in the density of cells and percentage of water content, in refractive index and absorption coefficient. This helps increase the sensitivity and precision of early melanoma diagnosis [13].

3.5.2. Methylation method

Methylation can also be used for improving THz detection quality of melanoma, which is a competitive and noninvasive method. The methylation causes water molecules to reorganize around the methyl groups, changing the rigidity and the shell dynamics of hydration. Hypermethylation patterns were detected under THz spectroscopy for the methylated DNA from melanoma cells. These amplify the contrast of the THz signal between methylated melanoma tissues and methylated normal tissues. The differentiation between methylated and non-methylated DNA regions has more than 90% accuracy. It bypasses the penetration limits mentioned above and aids the surgeries that excise the melanoma [14].

4. Challenges and future directions

4.1. Tradeoffs of overall THz imaging quality

THz imaging faces many challenges that prevent it from biomedical applications. First, for every extra requirement in resolution, there is an increase in destabilization. These two limitations restrict the overall imaging quality in biomedical practice.

4.1.1. Destabilization

One of the main challenges of THz imaging is the high response to disturbance. Not only does the previously mentioned limited penetration depth contribute to destabilization, but the THz radiation also has significant absorption and scattering in biological tissues, causing high signal loss and reduced image quality. The existence of water vapor absorption in the THz spectrum decreases the quality of the signal, and a small fluctuation in temperature offers a magnificent change in the imaging result [15].

4.1.2. Low resolution

The other challenge is low resolution. The signal attenuation hinders clinical diagnosis applications [16]. The latest studies exceed the traditional diffraction limits of THz and have achieved sub-wavelength resolution (~40 nm), but it is still hindered by a high ratio of signal to noise in water-abundant tissues [17].

4.2. Low acquisition speed

The acquisition speed of THz imaging is relatively slow compared to traditional imaging techniques such as CT and MRI. The imaging system depends on the mechanical delay lines with pulsed imaging, resulting in around 10 seconds per image [16]. For improved ratio of signal to noise by averaging multiple scans, the acquisition speed is as low as 30 seconds for more advanced images [18]. It makes THz imaging hard to detect dynamic tissues, such as tissues with blood flow. This limits its use in

real-time imaging applications and makes it challenging to present dynamic processes in biological tissues.

4.3. Lack of enough experimental data

The main challenges that block the THz application of clinical diagnosis are the lack of comparable experimental data. It can be seen through the small sample size and the lack of standardization of THz imaging.

Many THz studies are cutting-edge and experimental, rely more on ex vivo and animal tissues, and are thus limited in sample size. Therefore, the findings may not generalize to in vivo experiments and broader populations. 72% of THz studies use fewer than 30 patient samples, while most MRIs have more than 100 participants (90% of MRI studies of breast cancer had more than 500 participants) [19].

The lack of standardization also hinders application. There are 14 proprietary software tools in 62 studies of THz imaging. These tools have disparate data formats, which create barriers to resampling validation and clinical applications [20].

4.4. Future directions

Despite these challenges, THz imaging is promising for biomedical applications. Advances in THz technology, such as detection with metallic tips, single-pixel cameras and hybrid systems [18], have the potential to improve the acquisition speed and enable real-time imaging. Integrating THz imaging with other imaging methods can offer a more comprehensive view of biological tissues. Further research in nanoparticles and near THz waves is also essential for balancing between sensitivity and robustness, improving THz imaging technology, and expanding its applications in biomedicine.

5. Conclusion

Terahertz imaging is a rapidly evolving technology with great potential for biomedical applications. Its unique advantages, being sensitive and non-invasive, make it suitable for its medical applications, especially in cancer detection. Although there are still some limitations to overcome, including high response to disturbance, low resolution, slow acquisition speed, small sample size, and the lack of standardization, recent advances in terahertz technology show great promise in addressing these challenges.

The future of terahertz imaging lies in the continued development of new sources, detectors, and imaging technologies, as well as the future popularized clinical practice. The standardization of terahertz imaging technology is also crucial for its wide application in clinical practice. With further research and development, terahertz imaging has the potential to become an important tool for biomedical diagnosis and treatment, improving patient outcomes and quality of life.

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